3D model fitting for facial expression analysis under uncontrolled imaging conditions

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Abstract

This paper addresses the recovering of 3D pose and animation of the human face in a monocular single image under uncontrolled imaging conditions. Our goal is to fit a 3D animated model in a face image with possibly large variations of head pose and facial expressions. Our data were acquired from filmed epileptic seizures of patients undergoing investigation in the videotelemetry unit, La Timone hospital, Marseille, France.

1. Introduction

Facial expression analysis has been an active research topic for behavioral scientists and psychologists since the work of C. Darwin in 1872 [4, 7]. In 1978, Suwa et al. [11] presented a preliminary investigation on automatic facial expression analysis by tracking the motion of several identified spots on an image sequence. Since then considerable progress has been made in building computer systems that attempt to automatically analyze and recognize facial motions [8, 10].

Two principal classes of approaches have been developed: Image-based [2, 9] and Model-based approaches [5, 6]. Image-based methods extract features from images without relying on elaborate knowledge about the object of interest. Their principal quality is their quickness and simplicity. However, if the data images are very diverse (e.g., variation of illumination, of view, of head pose) image-based approaches can become erratic and unsatisfactory. On the other hand model-based methods use models which maintain the essential characteristics of the face (position of the eyes relative to the nose for example), but which can deform to fit a range of possible facial shapes and expressions.

1 We thank O. Faugeras for suggesting the topic of this article and facilitating the collaboration.
Figure 1. The Candide face model

these deformation vectors).

Figure 2. one example of a shape unit, and four examples of animation units

For our work we had to slightly modify the original model, principally in order to remove the top part of the head and to add some specific animation units. These modifications were motivated by the specificity of our images. The patients in fact wore EEG electrodes on the head and the forehead was often hidden. Furthermore, the expressions encountered during the crises were often asymmetric and some additional animation parameters were necessary to cover all the scope of the possible expression.

2.2. The Reference Texture

We also added a reference texture to the model. This texture has been computed as the average between a few number of faces on which the model has been manually placed. Fig.3 shows this reference texture on the model.

3. Model Fitting

3.1. Energy

For a new image of a face, we want to find the best position of the 3D model and the best values of the shape and animation parameters in the sense that the projection of the mesh in the image matches the face (see Fig.4). Let us define an energy which measures the quality of a given position of the 3D model (and its projection). We use the cross-correlation between the reference texture, $I_{ref}$, and the image in which we want to fit the model, $I$. The support of the cross correlation is, for each vertex $P_i$, the set of triangles $T_j$ incidents to this vertex (see Fig.5).

$$\rho_i = \sum_{j|P_i \in T_j} \int_{T_{ref,j}} (I_{ref}(P) - \overline{I_{ref,i}}) (I(\varphi(P)) - \overline{I_{\varphi,i}}) dP$$

with

$$\overline{I_{ref,i}} = \frac{1}{\sum_{j|P_i \in T_j} |T_{ref,j}|} \sum_{j|P_i \in T_j} \int_{T_{ref,j}} I_{ref}(P) dP$$

$$\overline{I_{\varphi,i}} = \frac{1}{\sum_{j|P_i \in T_j} |T_{ref,j}|} \sum_{j|P_i \in T_j} \int_{T_{ref,j}} I(\varphi(P)) dP$$

Let us then define:

$$\langle I_{ref}, I \rangle_{\varphi} = \sum_{i=0}^{n} \rho_i$$

where $n$ is the number of points in the model.

And finally the energy:
\[ \rho_{I, \varphi}(M) = \frac{\langle I_{\text{ref}}, I \rangle_{\varphi}}{\sqrt{\langle I_{\text{ref}}, I_{\text{ref}} \rangle} \sqrt{\langle I, I \rangle_{\varphi}}} \]

\( \varphi \) is a bijection from \( I_{\text{ref}} \) to \( I \) based on the current projection of the model (see Fig. 5).

Figure 5. support of the cross correlation and \( \varphi \), the bijection between the reference texture and the current projection of the model in the image.

This energy has the advantage of being invariant to any affine transformation of the histogram of the image.

3.2. Energy minimization

We computed the derivatives of the energy \( \rho_{I, \varphi}(M) \) with respect to the 3D global position of the model, and to the shape and animation parameters. We then perform a multi-scale gradient descent: we use a quasi-Newton method with non-linear constraints.

The multi-scale method makes the process less dependent on the initialization of the minimization and quicken the convergence. The constraints imposed in the minimization algorithm are: limits on the shape and animation parameters, some specific conditions on the mesh (e.g.: the eyelids and the lips must not pass through each other) and the fact that the projection of the mesh should not exceed the borders of the image.

4. Facial Expression

Once the model is fitted in an initial image of a subject, we define a new reference texture using the image and the projection of the fitted model. Given a new image of the same subject with a new facial expression, we use this new reference texture in order to fit the model in this image. The minimization is now done only with respect to global position and animation parameters (the shape parameters are supposed to be constant for two images of the same person). The facial expression can then be represented as the variation of the animation parameters between the neutral image of the subject and the expressive one.

5. Results

During seizures, large movements can occur and occlusion of the image may be produced by intervention of medical personnel. Therefore we manually selected several images for each patient: one of a neutral expression and some during seizures. Fig. 7 shows some of the results of the algorithm: the selected images and the final fit of the 3D model.

Once the model is fitted on the neutral image and on the expressive one, we can compute the variation of the animation parameters from the first image to the second one and for example apply that variation to another position of the model (Fig. 8).

6. Conclusion

We have proposed a method to fit a 3D animated model in a monocular single image under uncontrolled imaging conditions. Our method is based on an energy defined with a cross-correlation term and an energy minimization process. We fitted the model on real-world data obtained in a medical framework. The principal drawback of our approach is the time of computation of the optimization process which is quite far from real-time. However real-time processing was not one of our requirements, since our work was motivated by a need for an analysis tool. Further work includes investigating on the potential clinical use of this tool and on a more sophisticated model (such as including more advanced texture statistics than just an average).

Written informed consent was obtained from all patients for the use of their video recordings, including for publication.
References